

Competing growth mechanisms in the development of saccular aneurysms

Stress-driven growth and control laws

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The Geometry and Mechanics of Growth in Living Systems
Cargèse, July 14-26, 2008

Outline

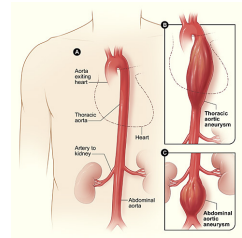
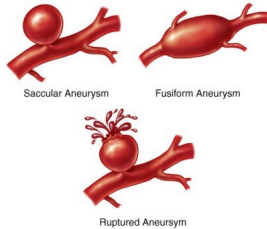
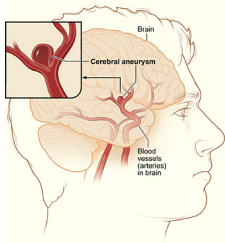
- 1 Histology and pathology
- 2 Mechanical model
 - Geometry & kinematics
 - Working & balance
 - Constitutive issues
 - Discussion
- 3 Multiple growth mechanisms
 - Mechanical model
 - Biomechanical characterisation
- 4 Numerical simulations

Part I

Saccular aneurysms

1 Histology and pathology

Aneurysms



Saccular (sac-like), with a well-defined neck.



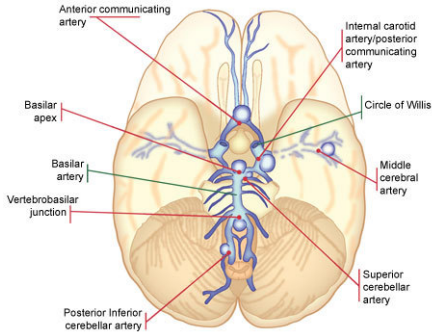
Broad-based with a wide neck.



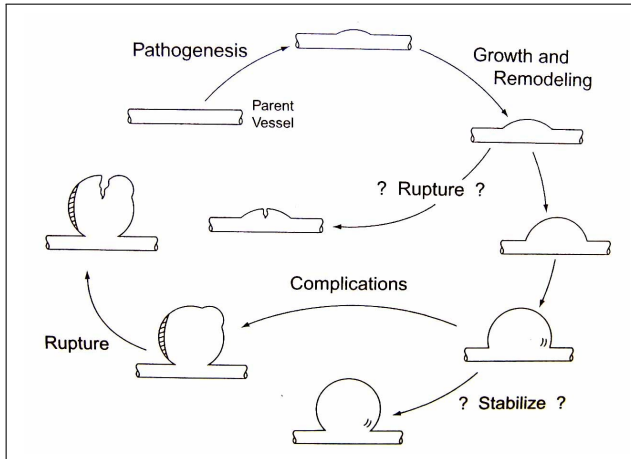
Fusiform (spindle shaped) without a distinct neck.

Aneurysms

Intracranial saccular aneurysms are pouches of the arterial wall.



Aneurysms



[J.D. Humphrey, *Cardiovascular Solid Mechanics*, 2001]

Aneurysms

	Time scale of development					Clinical presentation			
	Days–Months		Years	Decades	Multiple (148 aneurysms)	Single (232 aneurysms)	With SAH (30 aneurysms)	Total (380 aneurysms)	
					Mean follow up (months)				
					13.3	11.8	14.2	13.8	
Type 1									
Type 2					3 (2.0%)	1 (0.4%)		4 (1.0%)	
Type 3					9 (6.1%)	9 (3.9%)	4 (13.3%)	18 (4.7%)	
Type 4					136 (91.9%)	222 (95.7%)	26 (86.7%)	358 (94.2%)	

[M. Yonekura, *Neurologia medico-chirurgica*, 2004]

Part II

Mechanical model

- 2 Mechanical model
 - Geometry & kinematics
 - Working & balance
 - Constitutive issues
 - Discussion

Growth mechanics

Growth as change in the zero-stress state.

ex vivo

zero-load

zero-stress (?)

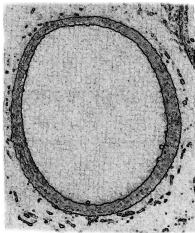
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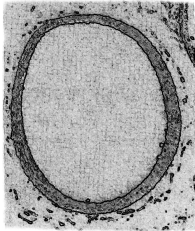


[Y. C. Fung, *Biomechanics: Mechanical Properties of Living Tissues*, 1993]

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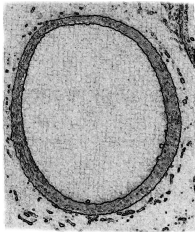
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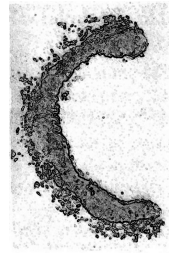
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Growth mechanics

Growth as change in the zero-stress state.

\mathcal{D}



\mathbf{p} : *gross placement*

$\nabla \mathbf{p}$: *gradient of the gross placement*

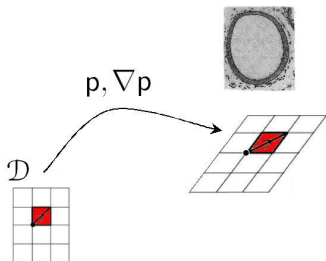
\mathbb{G} : *growth*

\mathbf{A} : *warp (purely elastic)*

(\mathbf{p}, \mathbb{G}) : *refined motion*

Growth mechanics

Growth as change in the zero-stress state.



p : *gross placement*

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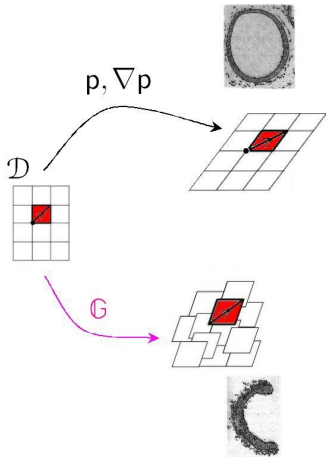
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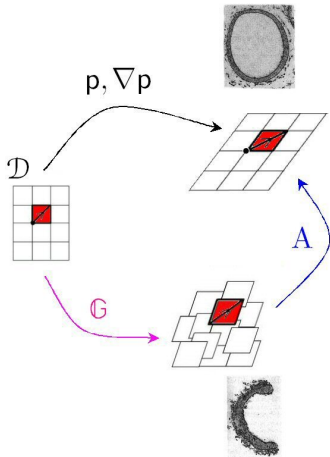
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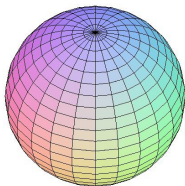
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Saccular aneurysms

paragon shape \mathcal{D} of the vessel

$$\mathcal{B}(x_0, \xi_+) - \bar{\mathcal{B}}(x_0, \xi_-)$$



spherical coordinates

$$\hat{\xi}(x), \hat{\vartheta}(x), \hat{\varphi}(x)$$

spherically symmetric vector fields

$$v(x) = v(\xi) \mathbf{e}_r(\vartheta, \varphi)$$

spherically symmetric tensor fields

$$L(x) = L_r(\xi) P_r(\vartheta, \varphi) + L_h(\xi) P_h(\vartheta, \varphi)$$

orthogonal projectors

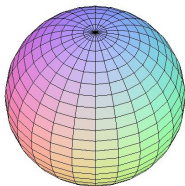
$$P_r := \mathbf{e}_r \otimes \mathbf{e}_r$$

$$P_h := I - P_r$$

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orthogonal projectors

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Geometry & kinematics

gross placement

$$\mathbf{p} = \mathbf{x}_0 + \rho \mathbf{e}_r$$

gradient of the gross placement

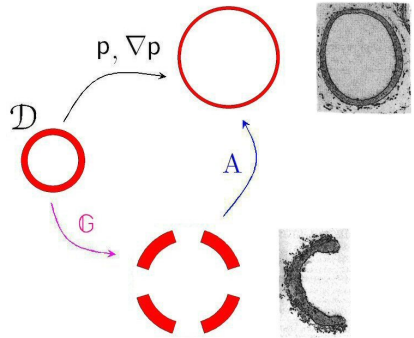
$$\nabla \mathbf{p} = \rho' P_r + \frac{\rho}{\xi} P_h$$

growth

$$\mathbb{G} = \gamma_r P_r + \gamma_h P_h$$

warp

$$\mathbb{A} := (\nabla \mathbf{p}) \mathbb{G}^{-1} = \alpha_r P_r + \alpha_h P_h$$



Geometry & kinematics

refined motion: (\mathbf{p}, \mathbb{G})

refined velocity: $(\dot{\mathbf{p}}, \dot{\mathbb{G}} \mathbb{G}^{-1})$

$$\dot{\mathbf{p}} = \dot{\rho} \mathbf{e}_r$$

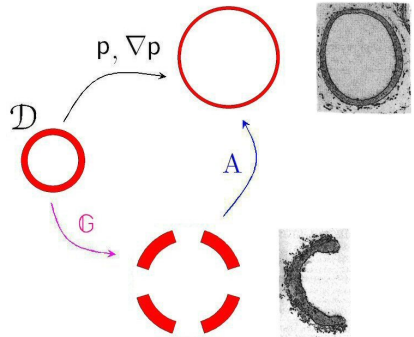
$$\dot{\mathbb{G}} \mathbb{G}^{-1} = \frac{\dot{\gamma}_r}{\gamma_r} \mathbf{P}_r + \frac{\dot{\gamma}_h}{\gamma_h} \mathbf{P}_h$$

test velocity: (\mathbf{v}, \mathbb{V})

$$\mathbf{v} = v \mathbf{e}_r$$

$$\mathbb{V} = V_r \mathbf{P}_r + V_h \mathbf{P}_h$$

(gross and *growth* velocity)



Working

Goal:

- To describe the energetic balance of **growth**

Working

- (brute) elasticity

$$\int_{\mathcal{D}} -\mathbf{S} \cdot \nabla \mathbf{v} + \int_{\partial \mathcal{D}} \mathbf{t}_{\partial \mathcal{D}} \cdot \mathbf{v}$$

- **growth** + elasticity

$$\int_{\mathcal{D}} \left(\mathbf{Q}^i \cdot \mathbf{v} - \mathbf{S} \cdot \nabla \mathbf{v} \right) + \int_{\mathcal{D}} \mathbf{Q}^o \cdot \mathbf{v} + \int_{\partial \mathcal{D}} \mathbf{t}_{\partial \mathcal{D}} \cdot \mathbf{v}$$

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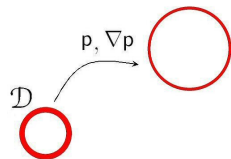
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Balance laws

balance of (*brute*) stress

$$2(S_r(\xi) - S_h(\xi)) + \xi S'_r(\xi) = 0$$

$$\mp S_r(\xi_{\mp}) = t_{\mp}$$

balance of *accretive stress*

$$Q_r^i(\xi) - Q_r^o(\xi) = 0$$

$$Q_h^i(\xi) - Q_h^o(\xi) = 0$$

Balance laws

balance of (*brute*) stress

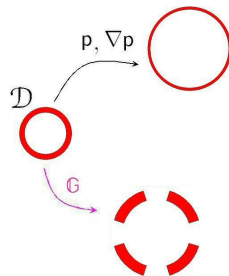
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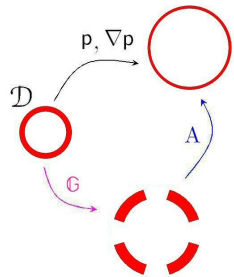
$$Q_r^i(\xi) - Q_r^o(\xi) = 0$$

$$Q_h^i(\xi) - Q_h^o(\xi) = 0$$



Characterising the passive mechanical response

- Energetics
- Dissipation principle



Energetics

$$\Psi(\mathcal{P}) = \int_{\mathcal{P}} \mathbf{J} \psi, \quad \mathbf{J} := \det(\mathbf{G}) > 0$$

(H₁₁): the value of $\psi(x)$ depends solely on the value of the warp $\mathbf{A}(x)$

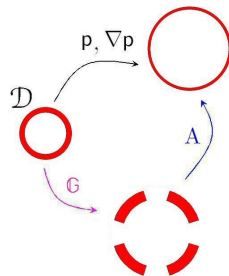
$$\psi(x) = \phi(\alpha_r(\xi), \alpha_h(\xi); \xi)$$

(H₁₂): incompressible elasticity

$$\det \mathbf{A} = \alpha_r \alpha_h^2 = 1$$

Fung strain energy density

$$\tilde{\phi}(\alpha) = (c/\delta) \exp((\Gamma/2)(\alpha^2 - 1)^2)$$



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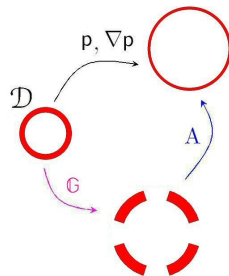
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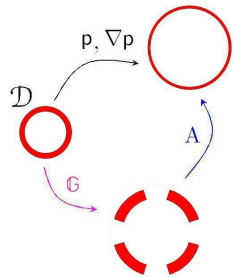
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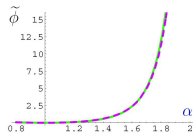
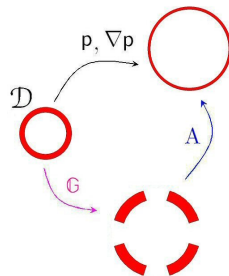
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Dissipation principle

$$\mathbf{S} \cdot \nabla \dot{\mathbf{p}} - \mathbf{Q}^i \cdot \dot{\mathbf{C}} \mathbf{G}^{-1} - (\mathbf{J} \tilde{\phi}) \cdot \dot{\mathbf{C}} \geq 0$$

$$\left(\mathbf{S} \mathbf{G}^T - \mathbf{J} \frac{d\tilde{\phi}}{d\mathbf{A}} \right) \cdot \dot{\mathbf{A}} - \left(\mathbf{Q}^i - \mathbf{A}^T \mathbf{S} \mathbf{G}^T + \mathbf{J} \tilde{\phi} \mathbf{I} \right) \cdot \dot{\mathbf{C}} \mathbf{G}^{-1} \geq 0$$

consistency

$$\mathbf{S} = \mathbf{J} \frac{d\tilde{\phi}}{d\mathbf{A}} \mathbf{G}^{-T} + \overset{+}{\mathbf{S}}, \quad \mathbf{Q}^i = \mathbf{A}^T \mathbf{S} \mathbf{G}^T + \mathbf{J} \tilde{\phi} \mathbf{I} + \overset{+}{\mathbf{Q}}^i$$

reduced dissipation inequality

$$\overset{+}{\mathbf{S}} \mathbf{G}^T \cdot \dot{\mathbf{A}} - \overset{+}{\mathbf{Q}}^i \cdot \dot{\mathbf{C}} \mathbf{G}^{-1} \geq 0$$

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Mechanical model

Kinematics

gross placement

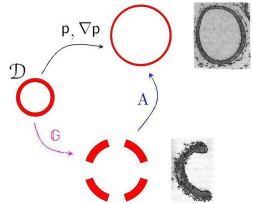
$$\mathbf{p} = \mathbf{x}_o + \rho \mathbf{e}_r$$

growth

$$\mathbf{G} = \gamma_r \mathbf{P}_r + \gamma_h \mathbf{P}_h$$

warp

$$\mathbf{A} = \alpha_r \mathbf{P}_r + \alpha_h \mathbf{P}_h$$



Working

$$\int_{\mathcal{D}} \left(\mathbf{Q}^i \cdot \mathbf{v} - \mathbf{S} \cdot \nabla \mathbf{v} \right) + \int_{\mathcal{D}} \mathbf{Q}^o \cdot \mathbf{v} + \int_{\partial \mathcal{D}} \mathbf{t}_{\partial \mathcal{D}} \cdot \mathbf{v}$$

(Reduced) dissipation inequality

$$\overset{+}{\mathbf{S}} \mathbf{G}^T \cdot \dot{\mathbf{A}} - \overset{+}{\mathbf{Q}}^i \cdot \dot{\mathbf{G}} \mathbf{G}^{-1} \geq 0$$

$$\overset{+}{S} \mathbb{G}^T \cdot \dot{\mathbb{A}} - \overset{+}{Q}^i \cdot \dot{\mathbb{G}} \mathbb{G}^{-1} \geq 0$$

In this framework, in a homeostatic state ($\mathbb{G} = \text{stat.}$), **no dissipation is associated with growth.**

$$\dot{S} \mathbb{G}^T \cdot \dot{A} - \dot{Q}^i \cdot \dot{\mathbb{G}} \mathbb{G}^{-1} \geq 0$$

In this framework, in a homeostatic state ($\mathbb{G} = \text{stat.}$), **no dissipation is associated with growth.**

But...

Even if the relaxed configuration does not evolve, some energy may be dissipated.

How to explain that?
How to deal with that?

Part III

Multiple growth mechanisms

- 3 Multiple growth mechanisms
 - Mechanical model
 - Biomechanical characterisation

Multiple (competing) growth mechanisms

(s) *slipping*, (c) *recovery*, and (t) *tissue apposition/resorption*

$$\mathbb{G} = \mathbb{G}_t \mathbb{G}_c \mathbb{G}_s$$

s sliding of tissue constituents

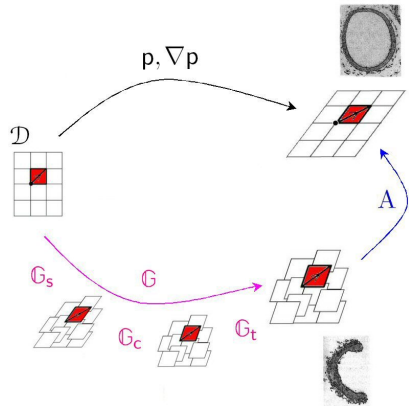
passive

c any action directly
contrasting the slipping

active

t fiber deposition/removal,
cell proliferation/destruction

active



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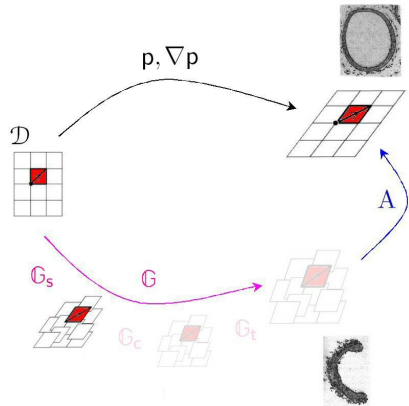
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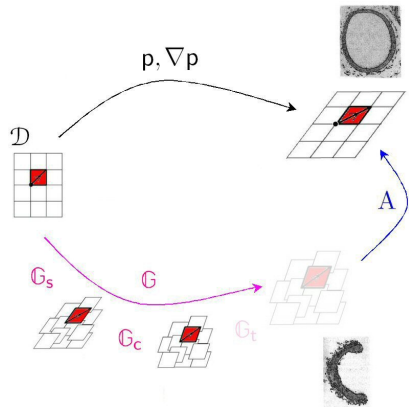
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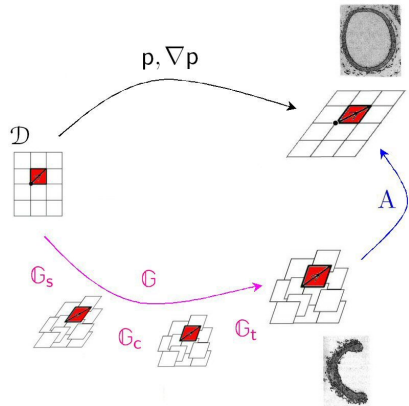
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active



Multiple (competing) growth mechanisms

(s) *slipping*, (c) *recovery*, and (t) *tissue apposition/resorption*

$$\mathbb{G} = \mathbb{G}_t \mathbb{G}_c \mathbb{G}_s$$

s sliding of tissue constituents

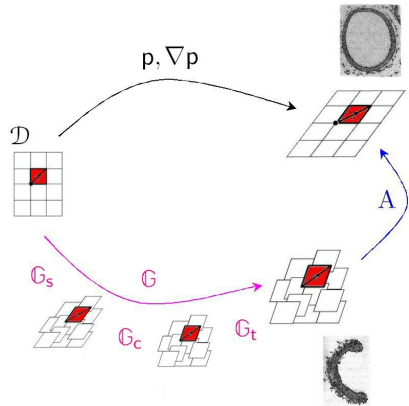
passive

c any action directly
contrasting the slipping

active

t fiber deposition/removal,
cell proliferation/destruction

active



Multiple (competing) growth mechanisms

(s) *slipping*, (c) *recovery*, and (t) *tissue apposition/resorption*

$$\mathbb{G} = \mathbb{G}_t \mathbb{G}_c \mathbb{G}_s$$

growth velocity

$$\dot{\mathbb{G}} \mathbb{G}^{-1} = \dot{\mathbb{G}}_t \mathbb{G}_t^{-1} + \dot{\mathbb{G}}_c \mathbb{G}_c^{-1} + \dot{\mathbb{G}}_s \mathbb{G}_s^{-1}$$

test velocity

$$\mathbb{V} = \mathbb{V}_t + \mathbb{V}_c + \mathbb{V}_s$$

working

$$\int_{\mathcal{D}} \left(\mathbb{Q}_t^i \cdot \mathbb{V}_t + \mathbb{Q}_c^i \cdot \mathbb{V}_c + \mathbb{Q}_s^i \cdot \mathbb{V}_s - \mathbb{S} \cdot \nabla \mathbf{v} \right) + \int_{\mathcal{D}} \left(\mathbb{Q}_t^o \cdot \mathbb{V}_t + \mathbb{Q}_c^o \cdot \mathbb{V}_c + \mathbb{Q}_s^o \cdot \mathbb{V}_s \right) + \int_{\partial \mathcal{D}} \mathbf{t}_{\partial \mathcal{D}} \cdot \mathbf{v}$$

Dissipation principle

$$\mathbf{S} \cdot \nabla \dot{\mathbf{p}} - \left(\mathbf{Q}_t^i \cdot \dot{\mathbf{G}}_t \mathbf{G}_t^{-1} + \mathbf{Q}_c^i \cdot \dot{\mathbf{G}}_c \mathbf{G}_c^{-1} + \mathbf{Q}_s^i \cdot \dot{\mathbf{G}}_s \mathbf{G}_s^{-1} \right) - (\mathbf{J} \tilde{\phi}) \cdot \geq 0$$

consistency

$$\mathbf{S} = \mathbf{J} \frac{d\tilde{\phi}}{d\mathbf{A}} \mathbf{G}^{-T} + \overset{+}{\mathbf{S}}$$

$$\mathbf{Q}_{\bullet}^i = \left(\mathbf{A}^T \mathbf{S} \mathbf{G}^T - \mathbf{J} \phi \mathbf{I} \right) + \overset{+}{\mathbf{Q}}_{\bullet}^i, \quad \bullet \in \{s, c, t\}$$

reduced dissipation inequality

$$\overset{+}{\mathbf{S}} \mathbf{G}^T \cdot \dot{\mathbf{A}} - \overset{+}{\mathbf{Q}}_t^i \cdot \dot{\mathbf{G}}_t \mathbf{G}_t^{-1} - \overset{+}{\mathbf{Q}}_c^i \cdot \dot{\mathbf{G}}_c \mathbf{G}_c^{-1} - \overset{+}{\mathbf{Q}}_s^i \cdot \dot{\mathbf{G}}_s \mathbf{G}_s^{-1} \geq 0$$

Dissipation principle

$$\mathbf{S} \cdot \nabla \dot{\mathbf{p}} - \left(\mathbf{Q}_t^i \cdot \dot{\mathbf{G}}_t \mathbf{G}_t^{-1} + \mathbf{Q}_c^i \cdot \dot{\mathbf{G}}_c \mathbf{G}_c^{-1} + \mathbf{Q}_s^i \cdot \dot{\mathbf{G}}_s \mathbf{G}_s^{-1} \right) - (\mathbf{J} \tilde{\phi})^\cdot \geq 0$$

consistency

$$\mathbf{S} = \mathbf{J} \frac{d\tilde{\phi}}{d\mathbf{A}} \mathbf{G}^{-\top} + \overset{+}{\mathbf{S}}$$

$$\mathbf{Q}_\bullet^i = \left(\mathbf{A}^\top \mathbf{S} \mathbf{G}^\top - \mathbf{J} \phi \mathbf{I} \right) + \overset{+}{\mathbf{Q}}_\bullet^i, \quad \bullet \in \{s, c, t\}$$

reduced dissipation inequality

$$\overset{+}{\mathbf{S}} \mathbf{G}^\top \cdot \dot{\mathbf{A}} - \overset{+}{\mathbf{Q}}_t^i \cdot \dot{\mathbf{G}}_t \mathbf{G}_t^{-1} - \overset{+}{\mathbf{Q}}_c^i \cdot \dot{\mathbf{G}}_c \mathbf{G}_c^{-1} - \overset{+}{\mathbf{Q}}_s^i \cdot \dot{\mathbf{G}}_s \mathbf{G}_s^{-1} \geq 0$$

Multiple (competing) growth mechanisms

(s) *slipping*, (c) *recovery*, and (p) *tissue apposition*

$$\mathbb{G} = \mathbb{G}_t \mathbb{G}_c \mathbb{G}_s$$

growth velocity

$$\dot{\mathbb{G}} \mathbb{G}^{-1} = \dot{\mathbb{G}}_t \mathbb{G}_t^{-1} + \dot{\mathbb{G}}_c \mathbb{G}_c^{-1} + \dot{\mathbb{G}}_s \mathbb{G}_s^{-1}$$

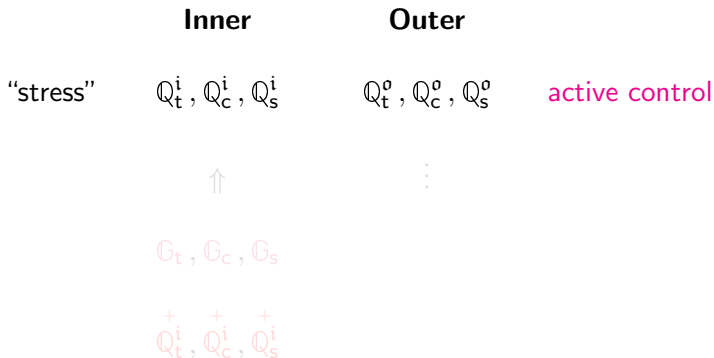
test velocity

$$\mathbb{V} = \mathbb{V}_t + \mathbb{V}_c + \mathbb{V}_s$$

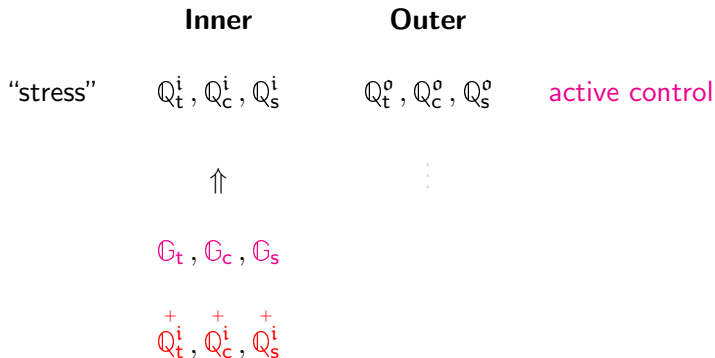
working

$$\int_{\mathcal{D}} \left(\mathbb{Q}_t^i \cdot \mathbb{V}_t + \mathbb{Q}_c^i \cdot \mathbb{V}_c + \mathbb{Q}_s^i \cdot \mathbb{V}_s - \mathbb{S} \cdot \nabla \mathbf{v} \right) + \int_{\mathcal{D}} \left(\mathbb{Q}_t^o \cdot \mathbb{V}_t + \mathbb{Q}_c^o \cdot \mathbb{V}_c + \mathbb{Q}_s^o \cdot \mathbb{V}_s \right) + \int_{\partial \mathcal{D}} \mathbf{t}_{\partial \mathcal{D}} \cdot \mathbf{v}$$

Characterising the accretive couples



Characterising the accretive couples



Characterising the accretive couples

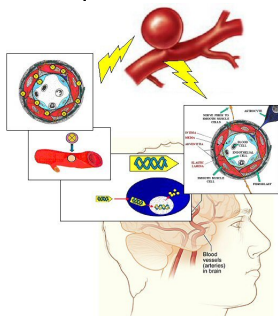
	Inner	Outer	
“stress”	Q_t^i, Q_C^i, Q_S^i	Q_t^o, Q_C^o, Q_S^o	active control



G_t, G_C, G_S

+ Q_t^i, Q_C^i, Q_S^i

⋮



Characterising the growth mechanisms

- (H2₁): We assume that only G_t changes volume, while neither G_s nor G_c affects volume
- (H2₂): We assume that tissue apposition is only radial

$$G_t = \gamma_r^t P_r + P_h$$

$$G_c = \gamma_r^c P_r + \gamma_h^c P_h$$

$$G_s = \gamma_r^s P_r + \gamma_h^s P_h$$

$$\gamma_r^c (\gamma_h^c)^2 = 1$$

$$\gamma_r^s (\gamma_h^s)^2 = 1$$

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$$\gamma_r^c (\gamma_h^c)^2 = 1$$

$$\gamma_r^s (\gamma_h^s)^2 = 1$$

Characterising the dissipation

(H3₁): We assume that dissipation is only due to growth

(H3₂): Linear viscous dissipation

$$\overset{+}{S} = 0$$

$$\overset{+}{Q}_t^i = -J D_r^t \dot{\gamma}_r^t / \gamma_r^t P_r$$

$$\overset{+}{Q}_c^i = -J (D_r^c \dot{\gamma}_r^c / \gamma_r^c P_r + D_h^c \dot{\gamma}_h^c / \gamma_h^c P_h)$$

$$\overset{+}{Q}_s^i = -J (D_r^s \dot{\gamma}_r^s / \gamma_r^s P_r + D_h^s \dot{\gamma}_h^s / \gamma_h^s P_h)$$

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$$\overset{+}{Q}_s^i = -J (D_r^s \dot{\gamma}_r^s / \gamma_r^s P_r + D_h^s \dot{\gamma}_h^s / \gamma_h^s P_h)$$

Evolution equations

growth

$$D^t \dot{\gamma}_r^t / \gamma_r^t = (T_r - \tilde{\phi}) + Q^t$$

$$D^c \dot{\gamma}_h^c / \gamma_h^c = (T_h - T_r) + Q^c$$

$$D^s \dot{\gamma}_h^s / \gamma_h^s = (T_h - T_r) + Q^s$$

$$Q_t^o / J = Q_r^t P_r$$

$$Q_c^o / J = Q_r^c P_r + Q_h^c P_h$$

$$Q_s^o / J = Q_r^s P_r + Q_h^s P_h$$

$$Q^t := Q_r^t$$

$$Q^c := (Q_h^c - Q_r^c)$$

$$Q^s := (Q_h^s - Q_r^s)$$

$$D^t := D_r^t$$

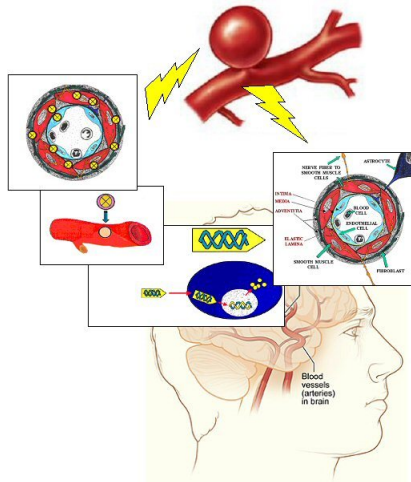
$$D^c := (2D_r^c + D_h^c)$$

$$D^s := (2D_r^s + D_h^s)$$

$$T_r = J^{-1} S_r \gamma_r \alpha_r$$

$$T_h = J^{-1} S_h \gamma_h \alpha_h$$

Characterising the controls



T_h^\diamond , T_r^\diamond : physiological “target” values.

Characterising the controls

(H4_s): null control on slipping mechanism

$$Q^s = 0$$

(H4_c): recovery tuned with respect to slipping

$$Q^c \sim G^c (T_h - T_r) + (1 - G^c) (T_h^\diamond - T_r^\diamond)$$

(H4_t): radial apposition driven by hoop stress

$$Q^t \sim G^t (T_h - T_h^\diamond)$$

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(H4_t): radial apposition driven by hoop stress

$$Q^t \sim G^t (T_h - T_h^\diamond)$$

$T_h^\diamond, T_r^\diamond$: physiological “target” values.

Evolution equations

gross motion

$$2(S_r(\xi) - S_h(\xi)) + \xi S_r'(\xi) = 0$$

$$\mp S_r(\xi_{\mp}) = t_{\mp}$$

growth

$$\dot{\gamma}_h / \gamma_h = \kappa_h (\Delta T_h - \Delta T_r)$$

$$\dot{\gamma}_r / \gamma_r = -2\dot{\gamma}_h / \gamma_h + \kappa_r \Delta T_h$$

$$\Delta T_h := T_h - T_h^{\diamond}$$

$$\kappa_h := (1/D^c + 1/D^s)(1 - G^c)$$

$$\Delta T_r := T_r - T_r^{\diamond}$$

$$\kappa_r := G^t / D^t$$

Part IV

Numerical simulations

- 4 Numerical simulations
 - Natural histories
 - Passive slipping, recovery, null tissue apposition
 - Passive slipping, slow recovery, tissue apposition

Simulated natural histories

- Let us assume that an aneurysm, subjected to a constant intramural pressure p^\diamond , has reached a spherical shape in a homeostatic state with hoop and radial stress:

$$T_h^\diamond, \quad T_r^\diamond.$$

- Let Q^\diamond be the value of the control Q^c necessary to maintain this homeostatic state:

$$Q^\diamond \sim T_h^\diamond - T_r^\diamond.$$

- Thus, let the intramural pressure experience a short-time bump:

$$p(t) = p^\diamond + \delta p(t).$$

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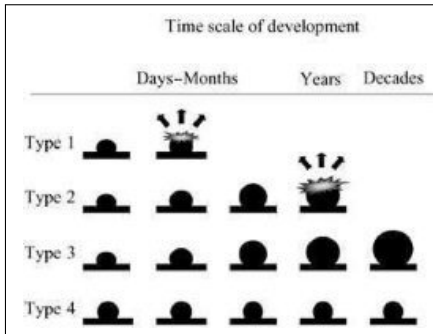
$$Q^\diamond \sim T_h^\diamond - T_r^\diamond.$$

- Thus, let the intramural pressure experience a short-time bump:

$$p(t) = p^\diamond + \delta p(t).$$

Simulated natural histories

- Efficient vs. Inefficient recovery
- Negligible vs. Non-negligible tissue apposition



History #1: slow recovery, null apposition

- 1 Q^c is held fixed to the previous value for the rest of the time:

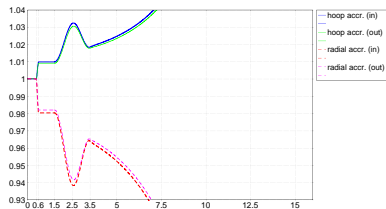
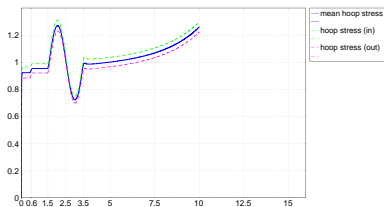
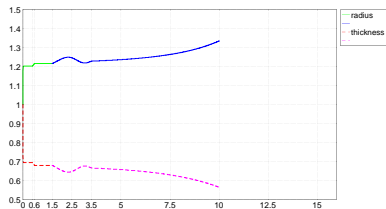
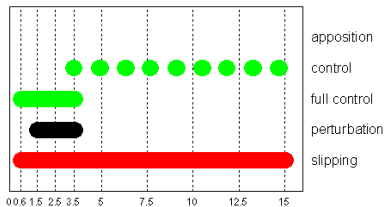
$$Q^c = Q^\diamond \sim T_h^\diamond - T_r^\diamond$$

simulating the inability of the recovery control to keep pace with a sudden perturbation

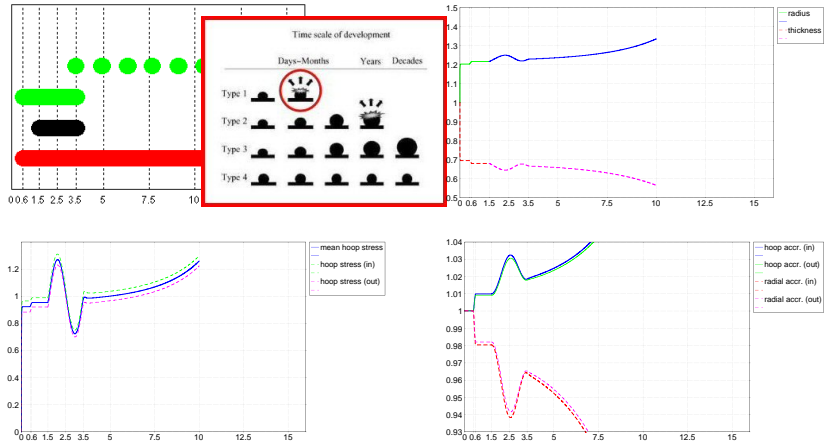
- 2 negligible tissue apposition:

$$Q^t \sim 0$$

SLOW RECOVERY ($G^c = 0$), null tissue apposition



SLOW RECOVERY ($G^c = 0$), null tissue apposition



History #2: fast recovery, null apposition

- 1 Q^c is set to a full recovery control:

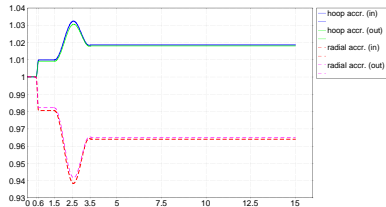
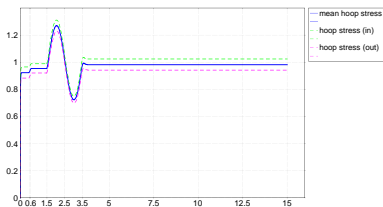
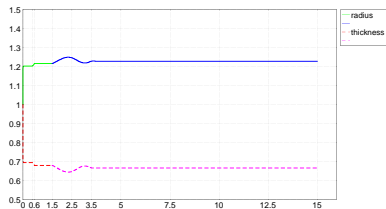
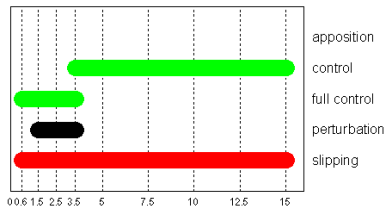
$$Q^c \sim T_h - T_r$$

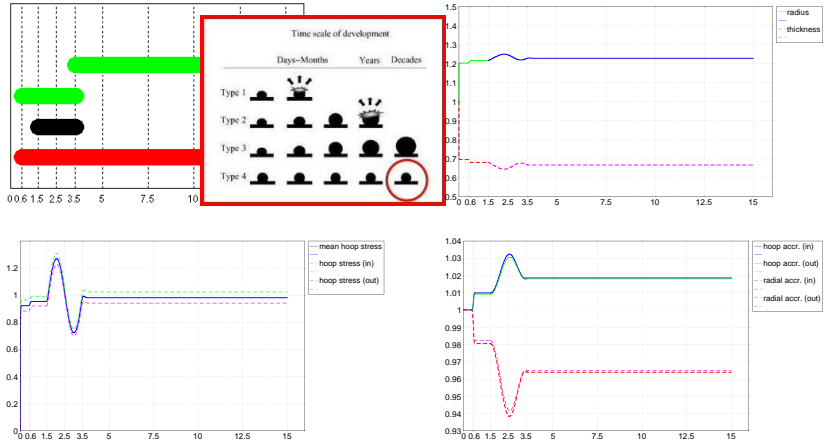
simulating the capability of the recovery control to immediately keep pace with a sudden perturbation

- 2 negligible tissue apposition:

$$Q^t \sim 0$$

FAST RECOVERY ($G^c = 1$), null tissue apposition



FAST RECOVERY ($G^c = 1$), null tissue apposition

History #3: delayed recovery, null apposition

- 1 Q^c is a fraction of the full recovery control:

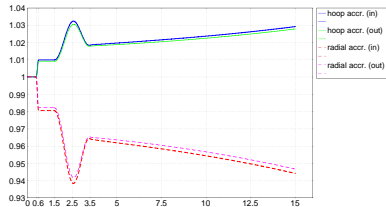
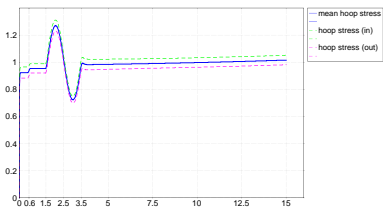
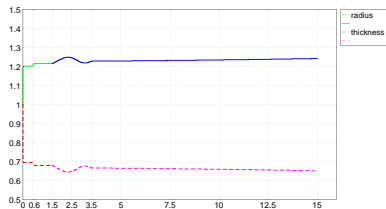
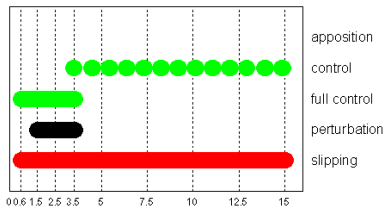
$$Q^c \sim G^c (T_h - T_r) + (1 - G^c) (T_h^\diamond - T_r^\diamond)$$

which is meant to simulate an impaired recovery control

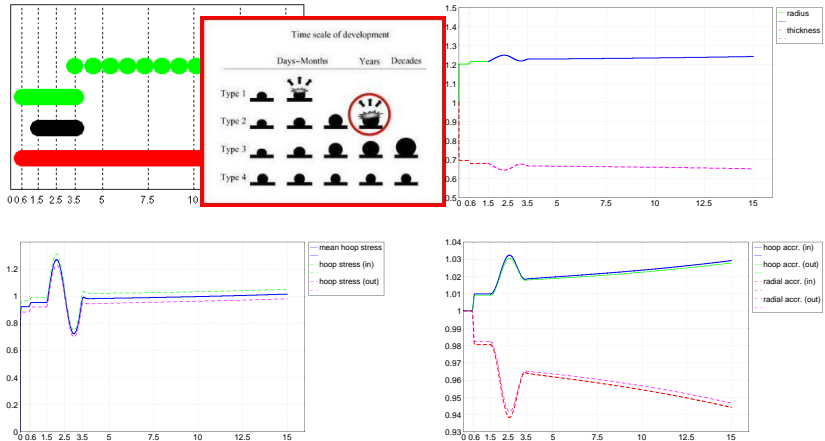
- 2 negligible tissue apposition:

$$Q^t \sim 0$$

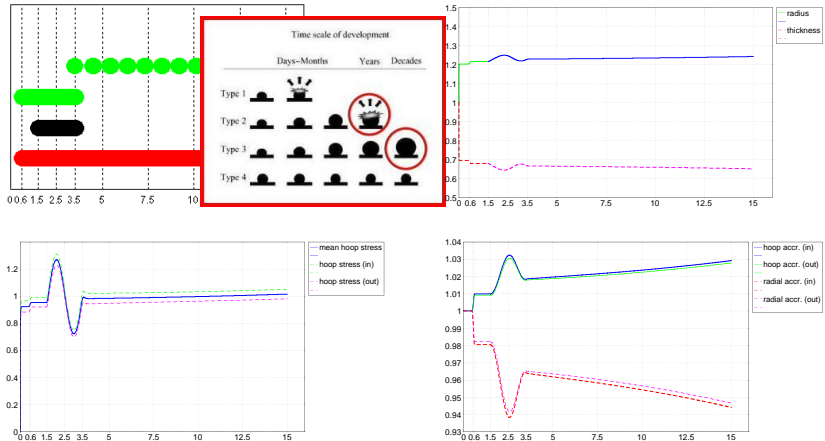
DELAYED RECOVERY ($G^c = 0.8$), null tissue apposition



DELAYED RECOVERY ($G^c = 0.8$), null tissue apposition



DELAYED RECOVERY ($G^c = 0.8$), null tissue apposition



History #4: slow recovery, tissue apposition

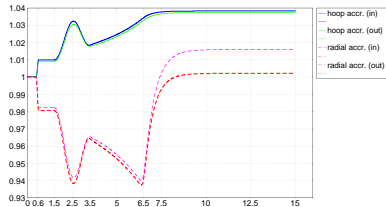
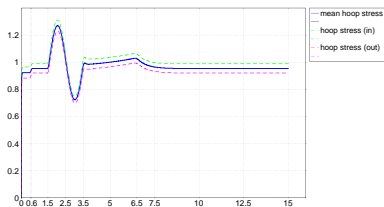
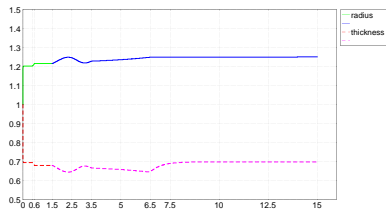
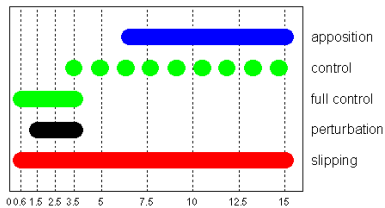
- 1 Q^c is held fixed to the previous value for the rest of the time:

$$Q^c(t) = Q^\diamond$$

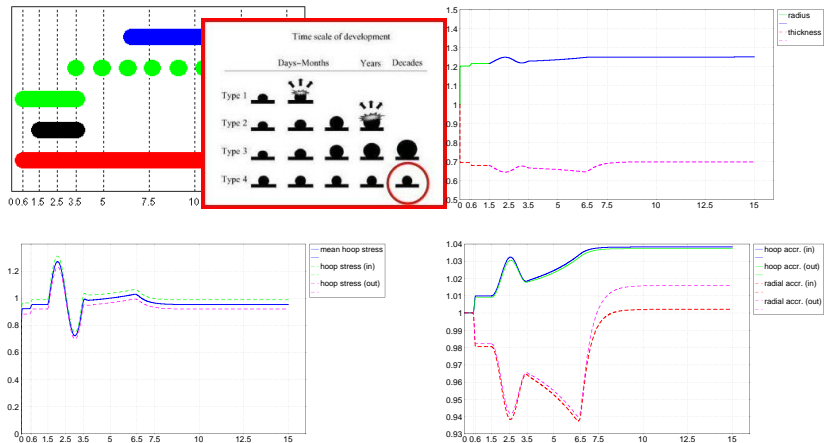
- 2 radial tissue apposition goes into action through a stress-driven control law:

$$Q^t \sim G^t(T_h - T_h^\diamond)$$

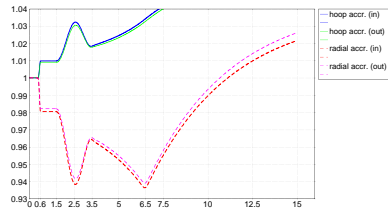
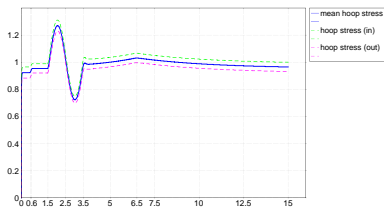
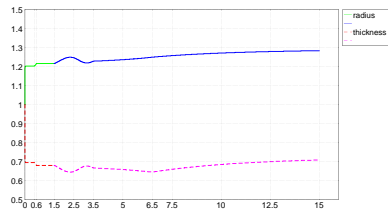
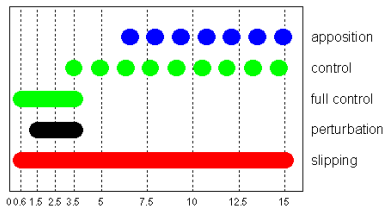
Slow recovery ($G^c = 0$), FAST TISSUE APPPOSITION ($G^t \gg 1$)



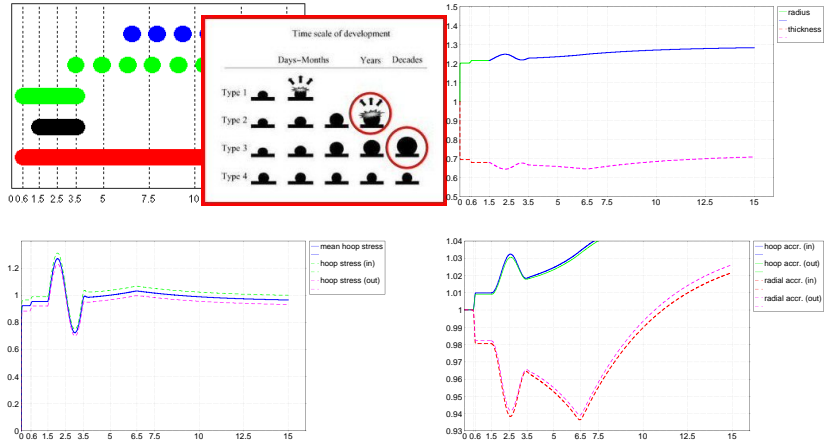
Slow recovery ($G^c = 0$), FAST TISSUE APPPOSITION ($G^t \gg 1$)



Slow recovery ($G^c = 0$), SLOW TISSUE APPPOSITION ($G^t \lll$)



Slow recovery ($G^c = 0$), SLOW TISSUE APPPOSITION ($G^t \lll$)



Summary

- Evolution of saccular aneurysms
 - elastic deformation;
 - growth, *i.e.* change of relaxed configuration.
- Multiple remodelling mechanisms
 - *slipping*: only passive;
 - *recovery*: slow/fast control;
 - *tissue apposition*: hoop stress driven control.
- Numerical evidence
 - recovery control is unable to maintain homeostatis;
 - tissue apposition plays a central role.

Future work

- In tight connection with biologists, physicists and clinicians...
- Better characterisation of the biological system
 - description of the growth mechanisms;
 - evolution of elastic properties;
 - non uniform material properties.
- Weaker assumptions on symmetry
- Quantitative calibration and model validation

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References

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- ② A. DiCarlo, V. Sansalone, A. Tatone, and V. Varano, Living Shell-Like Structures, in *Applied and Industrial Mathematics In Italy - II*, World Scientific, 2007.
 - First application to saccular aneurysms.
- ③ V. Sansalone, A. Tatone, V. Varano, and A. DiCarlo, Competing growth mechanisms in the development of saccular aneurysms, *in preparation*. (Ask me for preprint.)

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